

# **Apparatus and Method for Preparing Microparticles**

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## ***Background of the Invention***

### ***Cross-Reference to Related Applications***

This application is a continuation of application no. 09/438,659, filed November 12, 1999, the entirety of which is incorporated herein by reference. This application is related to co-pending application serial number 09/438,656, filed November 12, 1999, the entirety of which is incorporated herein by reference.

### ***Field of the Invention***

The present invention relates to preparation of microparticles. More particularly, the present invention relates to a method and an apparatus for preparing microparticles having a more controlled and symmetrical particle size distribution.

### ***Related Art***

A variety of methods is known by which compounds can be encapsulated in the form of microparticles. It is particularly advantageous to encapsulate a biologically active or pharmaceutically active agent within a biocompatible, biodegradable wall forming material (e.g., a polymer) to provide sustained or delayed release of drugs or other active agents. In these methods, the material to be encapsulated (drugs or other active agents) is generally dissolved, dispersed, or emulsified, using stirrers, agitators, or other dynamic mixing techniques, in a solvent containing the wall forming material. Solvent is then removed from the microparticles and thereafter the microparticle product is obtained.

Development of a microencapsulation process suitable for commercial scale production typically requires scaling up, by multiple factors, a laboratory scale process and/or a pilot scale process. The scaled-up process will almost always require larger piping and higher flow rates, particularly when the scale factor is very large or if it is desired or necessary to keep process transfer times similar to the smaller scale processes.

Scale-up into new, larger equipment is often unpredictable and achieved in large measure through trial and error. However, the economic costs of large-scale trial and error experiments can be prohibitive.

One approach to aiding the scale-up process is to use a static mixer to form an emulsion, as disclosed in U.S. Patent No. 5,654,008. In the method disclosed in U.S. Patent No. 5,654,008, a first phase, comprising the active agent and the polymer, and a second phase are pumped through a static mixer into a quench liquid to form microparticles containing the active agent. The use of a static mixer to form the emulsion tends to make the scale-up more predictable and reliable than the scale-up of other dynamic-mixing processes for making microparticles. However, numerous trials and experiments are still required to completely and accurately scale-up, such as to commercial scale or by a factor of 20 or more, a process such as the one disclosed in U.S. Patent No. 5,654,008.

For a commercial scale process, it is particularly important to control the distribution of the size of the microparticles to minimize yield losses. For example, microparticles, particularly controlled release microparticles containing an active agent or other type of substance to be released, can range in size of from about 25  $\mu\text{m}$  to about 250  $\mu\text{m}$  in diameter. For a particular commercial product, the useful or desired microparticle size range can be in the range of, for example, 25-150  $\mu\text{m}$ . Even in an efficient commercial production process, some percentage of the microparticles produced will be larger than the upper size limit, and some percentage of the microparticles produced will be smaller than the lower size limit, resulting in yield losses. Typically, the more narrow or tighter the desired microparticle size range, the larger the yield losses that result. These yield losses could be avoided or minimized if a more narrow microparticle size distribution could be achieved. Narrowing the microparticle size distribution eliminates or significantly reduces the losses resulting from microparticles that fall outside of the desired microparticle size range.

Thus, there is a need in the art for an improved method and apparatus for preparing microparticles. There is a particular need in the art for an improved process that can control particle size distribution, and achieve a more narrow particle size

distribution. There is a further need in the art for an improved process that can be more quickly, reliably, and accurately scaled-up from a laboratory or pilot scale to a commercial scale. The present invention, the description of which is fully set forth below, solves the need in the art for such improved methods and apparatus.

### *Summary of the Invention*

The present invention relates to an apparatus and method for preparing microparticles. In one aspect of the invention, a method of preparing microparticles is provided. The method comprises:

- preparing a first phase, the first phase comprising an active agent and a polymer;
- 10 preparing a second phase;
- preparing a quench liquid;
- pumping the first phase and the second phase through a first static mixer to form an emulsion; and
- flowing the emulsion through a manifold that includes a plurality of static mixers
- 15 into the quench liquid whereby droplets of the emulsion form microparticles.

In a further aspect of the present invention, another method for preparing microparticles is provided. The method comprises:

- preparing a first phase, the first phase comprising an active agent and a polymer;
- preparing a second phase;
- 20 preparing a quench liquid;
- combining the first phase and the second phase in a first static mixer to form an emulsion, the emulsion forming an outflow of the first static mixer;
- dividing the outflow of the first static mixer to form at least two flow streams;
- flowing each of the at least two flow streams through a separate second static
- 25 mixer; and
- combining the at least two flow streams with the quench liquid whereby droplets of the emulsion form microparticles.

In a further aspect of the present invention, a method for controlling particle size distribution of microparticles is provided. The method comprises:

preparing a first phase, the first phase comprising an active agent and a polymer;  
preparing a second phase;  
preparing a quench liquid;  
pumping the first phase and the second phase through a static mixing assembly to  
5 form an emulsion;

flowing the emulsion into the quench liquid whereby droplets of the emulsion  
form microparticles; and

adjusting a residence time of the emulsion in the static mixing assembly to obtain  
a predetermined particle size distribution of the resulting microparticles, wherein the  
10 residence time is equal to a length of the static mixing assembly divided by an average  
velocity of the emulsion through the static mixing assembly.

In yet a further aspect of the present invention, a microencapsulated active agent  
prepared by a method for preparing microparticles is provided. Such a method  
comprises:

15 preparing a first phase, the first phase comprising an active agent and a polymer;  
preparing a second phase;  
preparing a quench liquid;  
pumping the first phase and the second phase through a first static mixer to form  
an emulsion; and

20 flowing the emulsion through a manifold that includes a plurality of static mixers  
into the quench liquid whereby droplets of the emulsion form microparticles.

In yet a further aspect of the present invention, a microencapsulated active agent  
prepared by another method for preparing microparticles is provided. Such a method  
comprises:

25 preparing a first phase, the first phase comprising an active agent and a polymer;  
preparing a second phase;  
preparing a quench liquid;  
combining the first phase and the second phase in a first static mixer to form an  
emulsion, the emulsion forming an outflow of the first static mixer;

dividing the outflow of the first static mixer to form at least two substantially identical flow streams;

flowing each of the at least two substantially identical flow streams through a separate second static mixer; and

5 combining the least two substantially identical flow streams with the quench liquid whereby droplets of the emulsion form microparticles.

In still a further aspect of the present invention, a system for preparing microparticles is provided. The system includes a first and second pump, and a first static mixer in fluid communication with each of the pumps. One of the pumps is  
10 configured to pump an organic phase into the first static mixer. One of the pumps is configured to pump a continuous phase into the first static mixer. A manifold, comprising a plurality of static mixers, is in fluid communication with the first static mixer. An extraction vessel is in fluid communication with the manifold. The outflow of the first static mixer flows through the manifold into the extraction vessel. The plurality  
15 of static mixers in the manifold can be configured in parallel or in series.

### ***Features and Advantages***

It is a feature of the present invention that it can be used to prepare microparticles, including microparticles containing an active agent.

A significant advantage of the present invention is that it provides a method for  
20 controlling particle size distribution. By controlling particle size distribution, yield losses, resulting from microparticles that fall outside of a desired microparticle size range, can be substantially reduced or eliminated. This makes the present invention particularly useful for commercial products.

The present invention also advantageously allows for use of a more narrow or  
25 tighter target microparticle size range than in conventional processes. Narrowing the limit for the microparticle size range typically results in larger yield losses. These yield losses can be avoided or minimized by achieving a more narrow microparticle size distribution through the process of the present invention.

The present invention provides a method and apparatus that are particularly advantageous for scale-up. The parallel path manifold of the present invention allows for capacity increases from an established (single path) system without full-scale trial and error experiments in new and different equipment. The total flow rate can be increased from the single path system based upon the number of flow streams in the manifold.

### ***Brief Description of the Figures***

The present invention is described with reference to the accompanying drawings. In the drawings, like reference numbers indicate identical or functionally similar elements.

- 10       **FIG. 1** illustrates flow through a static mixer;  
          **FIG. 2** shows a static mixer suitable for use with the present invention;  
          **FIGS. 3A-3C** show various types or designs of static mixing elements;  
          **FIG. 4** depicts a graph of mass median diameter (microns) of microparticle size distribution as a function of average emulsion velocity (cm/min);  
15       **FIG. 5** depicts a graph of width of microparticle size distribution, as expressed by  $CoV_m$ , for various static mixers as a function of emulsion residence time (sec) in the static mixer;  
          **FIG. 6** depicts a graph of skewness of microparticle size distribution for various static mixers as a function of emulsion residence time (sec) in the static mixer; and  
20       **FIG. 7** shows an exemplary embodiment of an equipment configuration for preparing microparticles in accordance with the present invention.

### ***Detailed Description of the Preferred Embodiments***

#### ***Overview***

25       The present invention provides an improved method and apparatus for preparing microparticles. Maximum yield within a desired microparticle size range is an important aspect of any process or method for preparing microparticles. The size of the resulting microparticles is primarily controlled during the emulsification step of the process of the present invention. As will be explained in more detail below, the emulsification step uses

an in-line motionless or static mixer to create an emulsion from a first phase, comprising a polymer and a drug or other active agent, and a second phase, preferably an aqueous solution. The inventors of the present invention have unexpectedly found that the most dominant influential characteristic controlling the dispersity of microparticle size is the residence time of the emulsion in the static mixer before the emulsion is introduced to a quench or solvent-extraction liquid. Increased residence time in the emulsion-forming static mixer decreases polydispersity, and results in a more symmetrical particle size distribution.

The methods of the present invention use a static mixer to combine a first phase, comprising an active agent and a polymer, with a second phase to form an emulsion. The static mixer in which the first and second phases are combined to form the emulsion may be referred to herein as a "preblending static mixer". A process for forming an emulsion using a static mixer is described, for example, in U.S. Patent No. 5,654,008, the entirety of which is incorporated herein by reference. The phase comprising the active agent and the polymer may be referred to herein as the "organic phase". The other phase may be referred to herein as the "continuous phase".

The emulsion flowing out of the preblending static mixer flows through a manifold containing a plurality of static mixers into a quench liquid whereby droplets of the emulsion form microparticles. Alternatively, the outflow of the preblending static mixer is divided to form at least two flow streams. Each of the flow streams then flows through another separate static mixer. The flow streams are recombined downstream, and combined with the quench liquid whereby droplets of the emulsion form microparticles.

In a particularly preferred embodiment, the diameter of the preblending static mixer is greater than the diameter of the static mixers in the manifold, i.e., greater than the diameter of the static mixers through which the divided flow streams flow. When using a static mixer to form an emulsion, a variety of factors determine emulsion droplet size. Emulsion droplet size determines the size of the resulting microparticles. These factors include the density and viscosity of the various solutions or phases to be mixed, volume ratio of the phases, interfacial tension between the phases, static mixer

parameters (conduit diameter; length of mixing elements; number of mixing elements), and fluid velocity through the static mixer. The primary controlling variable is fluid velocity. Droplet size decreases as fluid velocity increases. Similarly, droplet size increases as fluid velocity (and pressure drop) decreases. Accordingly, the preblending static mixer is preferably larger in diameter than the static mixers in the manifold in order to handle the total flow from the feed streams (organic phase and continuous phase) at a lower velocity than the smaller diameter static mixers in the manifold.

In the present invention, a preblending static mixer is used to combine the organic phase and the aqueous phase to form the emulsion. In one embodiment, the emulsion is divided into a plurality of flow streams for flow through the manifold. The use of the preblending static mixer prior to the manifold is particularly advantageous because the organic phase and the aqueous phase are not immediately miscible or homogeneous, making the division of the combined flow stream problematic. For multiphase (e.g., oil/water) streams, the use of the manifold without the preblending static mixer could result in different compositions in each static mixer in the manifold. Because the combined organic and aqueous phases is not homogeneous, it would not divide evenly in conventional piping.

The manifold configuration of the present invention is particularly advantageous for scale-up. The parallel path manifold of the smaller diameter static mixers allows for capacity increases from an established (single path) system without full-scale trial and error experiments in new and different equipment. The total flow rate can be increased from the single path system based upon the number of flow streams in the manifold.

The present invention advantageously provides a method for controlling particle size distribution of microparticles. A first phase, comprising an active agent and a polymer, and a second phase are pumped through a static mixing assembly to form an emulsion. The emulsion flows into a quench liquid, whereby droplets of the emulsion form microparticles. By adjusting a residence time of the emulsion in the static mixing assembly, a predetermined particle size distribution of the resulting microparticles can be obtained. The residence time is equal to a length of the static mixing assembly divided by an average velocity of the emulsion through the static mixing assembly. The particle



size distribution can be narrowed by increasing the residence time. The particle size distribution can be broadened by decreasing the residence time. The residence time is preferably adjusted by changing the length of the static mixing assembly.

To ensure clarity of the description that follows, the following definitions are provided. By "microparticles" or "microspheres" is meant solid particles that contain an active agent or other substance dispersed or dissolved within a polymer that serves as a matrix or binder of the particle. The polymer is preferably biodegradable and biocompatible. By "biodegradable" is meant a material that should degrade by bodily processes to products readily disposable by the body and should not accumulate in the body. The products of the biodegradation should also be biocompatible with the body. By "biocompatible" is meant not toxic to the body, is pharmaceutically acceptable, is not carcinogenic, and does not significantly induce inflammation in body tissues. As used herein, "body" preferably refers to the human body, but it should be understood that body can also refer to a non-human animal body. By "weight %" or "% by weight" is meant parts by weight per total weight of microparticle. For example, 10 wt.% active agent would mean 10 parts active agent by weight and 90 parts polymer by weight. Unless otherwise indicated to the contrary, percentages (%) reported herein are by volume. By "controlled release microparticle" or "sustained release microparticle" is meant a microparticle from which an active agent or other type of substance is released as a function of time. By "mass median diameter" is meant the diameter at which half of the distribution (volume percent) has a larger diameter and half has a smaller diameter.

#### ***Method and Examples***

The following examples are provided to explain the invention, and to describe the materials and methods used in carrying out the invention. The examples are not intended to limit the invention in any manner.

### ***Example 1 - Static Mixer Tests***

A test program was conducted using a variety of static mixers. A static or motionless mixer consists of a conduit or tube in which is received a number of static mixing elements. Static mixers provide uniform mixing in a relatively short length of conduit, and in a relatively short period of time. With static mixers, the fluid moves through the mixer, rather than some part of the mixer, such as a blade, moving through the fluid. Flow through one type of static mixer is illustrated in Figure 1. A pump (not shown) introduces a stream of one or more fluids into a static mixer 10, as shown generally at 1. The stream is split and forced to opposite outside walls, as shown generally at 2. A vortex is created axial to the centerline of static mixer 10, as shown generally at 3. The vortex is sheared and the process recurs, but with the opposite rotation, as shown generally at 4. The clockwise/counterclockwise motion ensures a homogeneous product.

One example of a static mixer is shown in Figure 2. Static mixer 10 includes a number of stationary or static mixing elements 14 arranged in a series within a conduit or pipe 12. The number of static mixing elements can range from 4 to 32 or more. Conduit 12 is circular in cross-section and open at opposite ends 18 and 20 for introducing and withdrawing fluids. Mixing element 14 comprises segments 142. Each segment 142 consists of a plurality of generally flat plates or vanes 144. The two substantially identical segments 142 are preferably axially staggered with respect to each other. A static mixer as shown in Figure 2 is more fully described in U.S. Patent No. 4,511,258, the entirety of which is incorporated herein by reference.

Each of the static mixers tested displayed characteristic differences in design, length, diameter, and number of elements per length. A key aspect to the design of a static mixer is the geometry of the static mixing elements. The eight static mixers tested used three different types of static mixing elements: scissors elements; helical elements; and layered elements. A scissors mixing element, shown in Figure 3A, has two rows of baffles affixed perpendicular to each other, creating the impression of a pair of opened scissors. A helical mixing element, shown in Figure 3B, uses a 180° helical plane with a

90° offset and alternating direction of sequential elements. A layered element, shown in Figure 3C, uses corrugated sheets welded together to form open channels.

The characteristics of the eight static mixers tested are shown below in Table 1. The mixers ranged in size from 2½ inches in length with 5 mixing elements to 9¾ inches in length with 24 mixing elements. By arranging identical static mixers in series, the length and the number of mixing elements was increased; however, the number of mixing elements per unit length remained constant. The diameter of the static mixers tested ranged from ¼ inch to ½ inch.

Characteristics of the Test Mixers						
Mixer#	Diameter	Length	# of Elements	Element Design	Material	Manufacturer
1	¼"	6"	24	Helical	Plastic	Cole Palmer
2	¼"	9 ¾"	24	Helical	Stainless Steel	TAH
3	3/8"	4 ½"	12	Helical	Plastic	Cole Palmer
4	3/8"	9"	12	Helical	Stainless Steel	Kenics
5	3/8"	2 ½"	5	Layered	Stainless Steel	Koch
6	½"	5"	12	Helical	Plastic	TAH
7	½"	6"	12	Helical	Plastic	Cole Palmer
8	5/16"	2 7/8"	12	Scissors	Plastic	Omega

Table 1

One-hundred gram batches of 40% theoretically loaded risperidone microparticles were used to test the static mixers. A 16.7% polymer solution was prepared by dissolving 60 grams of MEDISORB® 7525 DL polymer (Alkermes, Inc., Blue Ash, Ohio) in ethyl acetate. A 28.6% drug solution was prepared by dissolving 40 grams of risperidone base (Janssen Pharmaceutica, Beerse, Belgium) in benzyl alcohol. The organic phase was prepared by mixing the drug solution into the polymer solution. The continuous or aqueous phase was a 1% polyvinyl alcohol (PVA) solution containing 6.5% ethyl acetate. The temperature of the organic and aqueous phases was 25°C. The ratio of the aqueous phase to the organic phase was 5:1. The quench liquid or extraction solution was an aqueous solution containing 2.5% ethyl acetate at 25°C. The ratio of the volume of extraction solution to batch size was 0.25 liters/gram.

The 100-gram batches were produced by forming an oil-in-water emulsion, and then extracting the solvent from the emulsion droplet to form a hardened polymer/drug microparticle. Two calibrated micropumps fed the static mixer under test, one micropump for the organic phase and one micropump for the aqueous phase. The  
5 micropumps were calibrated by monitoring total volume pumped over a timed period prior to the batch being run. A "Y" connection upstream of the static mixer under test was used to introduce the organic phase into the aqueous phase.

The static mixer under test discharged the resulting emulsion directly into an agitated extraction solution. The emulsion remained in the extraction solution for fifteen  
10 minutes to harden into microparticles. A sample of the resulting microparticles was tested using a Coulter LS230 Small Module particle size analyzer to determine particle size distribution. The flow rates were adjusted to target a mass median diameter of between about 30  $\mu\text{m}$  and 90  $\mu\text{m}$ . The experimental results for the eight static mixers tested is shown below in Table 2.

15

Summary of Experimental Results

Mixer					Process Conditions			Particle Data						
Number	Geometry	Diameter	Elements	Length	Total Flow	Cal. Velocity	Cal. Residence Time	Median	@ 84%	@ 16%	CoV <sub>m</sub>	Mean CoV <sub>m</sub>	Skewness	
		(in)	(#)	(in)	(ml/min)	(cm/min)	(sec)	( $\mu$ m)	( $\mu$ m)	( $\mu$ m)		( $\mu$ m)		
1	Helical	0.250	24	6.00	971	3068	0.298	24.60	43.88	6.07	1.54	25.45	0.666	0.259
1	Helical	0.250	24	6.00	464	1467	0.623	54.56	92.01	18.83	1.34	55.85	0.606	0.280
1	Helical	0.250	24	6.00	329	1039	0.880	87.76	159.10	33.30	1.43	97.33	0.667	0.346
2	Helical	0.250	24	9.75	960	3033	0.490	57.28	120.80	16.65	1.82	67.37	0.748	0.751
3	Helical	0.375	12	4.75	1140	1600	0.452	43.20	88.64	13.59	1.74	50.01	0.723	0.757
3	Helical	0.375	12	4.75	1213	1703	0.425	47.93	89.66	18.40	1.49	53.2	0.627	0.590
3	Helical	0.375	12	4.75	1215	1706	0.424	47.13	90.58	15.14	1.60	52.11	0.677	0.592
3	Helical	0.375	60	23.50	1133	1591	2.251	53.25	85.31	18.70	1.25	52.8	0.577	0.127
3	Helical	0.375	144	57.00	1036	1455	5.971	54.11	90.86	19.96	1.31	55.71	0.593	0.326
4	Helical	0.375	12	9.00	2792	3920	0.350	70.62	150.60	24.41	1.79	85.34	0.745	0.911
4	Helical	0.375	12	9.00	3527	4952	0.277	53.28	105.90	21.45	1.59	61.93	0.654	0.754
4	Helical	0.375	12	9.00	3703	5199	0.264	45.40	98.83	15.00	1.85	55.7	0.781	1.075
4	Helical	0.375	12	9.00	3487	4896	0.280	52.11	113.70	17.34	1.85	64.37	0.789	1.150
4	Helical	0.375	36	27.00	2888	4055	1.015	81.66	131.20	31.68	1.22	82.36	0.556	0.226
5	Layered	0.375	5	2.50	1166	1637	0.233	109.60	248.20	29.14	2.00	133.5	0.769	0.682
5	Layered	0.375	5	2.50	2423	3402	0.112	29.37	58.21	6.71	1.75	32.89	0.743	0.730
6	Helical	0.500	12	5.00	2764	2183	0.349	42.25	82.85	13.19	1.65	47.27	0.693	0.577
7	Helical	0.500	12	6.00	3929	3103	0.295	21.51	43.89	4.75	1.82	24.22	0.731	0.546
7	Helical	0.500	12	6.00	3507	2770	0.330	29.67	57.92	7.59	1.70	32.68	0.705	0.499
7	Helical	0.500	12	6.00	2684	2120	0.431	40.03	71.89	12.50	1.48	42.05	0.638	0.283
7	Helical	0.500	36	18.00	2779	2195	1.250	48.37	83.19	15.68	1.40	49.52	0.614	0.189
8	Scissors	0.313	12	2.88	909	1838	0.238	23.66	48.68	4.88	1.85	26.75	0.742	0.579
8	Scissors	0.313	12	2.88	620	1254	0.350	58.77	104.90	20.11	1.44	62.83	0.650	0.574

Table 2

The average emulsion velocity and residence time through a static mixer can be calculated from the flow rate into the static mixer and the length and diameter of the static mixer as follows:

- (1) Average Velocity = flow rate/cross-sectional area of empty static mixer
- (2) Residence Time = length of static mixer/Average Velocity

To characterize the particle size distribution, these parameters were measured: median, coefficient of variation of the median and skewness. The coefficient of variation of the median (CoV<sub>m</sub>) was used to characterize the span of the distribution.

$$(3) \text{CoV}_m = \frac{(\text{diameter of } \mu\theta \text{ at } 84\% - \text{diameter of } \mu\theta \text{ at } 16\%)}{\text{MMD}}$$

As the  $\text{CoV}_m$  approached zero, the distribution became more monodispersed.

The symmetry of the distribution was determined using the skewness coefficient. The

5 Coulter analyzer's method of determining skewness is as follows:

$$\text{Skewness} = \frac{\sum (n_c (x_c - x_a)^3)}{\text{SD}^3 \sum n_c}$$

$n_c$  = # of particles in c'th channel

$x_a$  = arithmetic mean of the distribution

$x_c$  = mean volume in the c'th channel

SD = standard deviation of the distribution

10 As the distribution became more symmetrical, the skewness approached zero. For right-skewed distributions (the particle size of the mode is less than the mean) the coefficient is positive; for left-skewed, the coefficient is negative.

Figure 4 shows the effect of the average emulsion velocity (cm/min) on the mass median diameter (MMD, microns) of the size distribution for the various static mixers under test. As shown in Figure 4, the MMD data for the plastic helical design mixer indicate a consistent well behaved inverse relationship between MMD and average velocity, independent of mixer diameter, length, and number of elements per length. The layered stainless steel (SS) mixer and the plastic scissors mixer also demonstrated an inverse relationship between MMD and average velocity. Figure 4 shows MMD data for a helical stainless steel (SS) mixer used to produce microparticles at the one kilogram scale, in a manner analogous to that described above for the 100 gram scale. The inverse relationship between MMD and average velocity was not readily apparent from the experimental data obtained with the stainless steel helical mixer at the one kilogram scale. Notably, this static mixer had the fewest elements per length (1.33 elements per inch) of all the static mixers tested.

Figure 5 shows the effect of emulsion residence time (sec) in the static mixer on the width of the microparticle size distribution ( $\text{CoV}_m$ ) using the various static mixers under test. An increase in residence time of the emulsion flowing through the static mixer causes a decrease in the width of the microparticle size distribution, until a minimum is reached. The data at extremely low residence times (less than one second)

have high variability, but consistently show an increase in the width of the particle size distribution as the residence time decreases below one second.

Figure 6 shows the effect of emulsion residence time (sec) in the static mixer on the skewness of the microparticle size distribution. As shown in Figure 6, as residence time increased, the skewness of the microparticle size distribution decreased. All of the distributions were right-skewed.

Experiments were also performed at the one kilogram scale, in a manner analogous to that described above for the 100 gram scale. However, for the one kilogram experiments, the number of static mixers was varied, using one, two, four, and eight static mixers arranged in series. The results of the one kilogram scale experiments are shown below in Table 3.

TABLE 3

Batch #	# of Mixers	Flow Rate (ml/min)	Cal. Velocity (cm/min)	Cal. Residence Time (sec)	Median (um)	@84% (um)	@16% (um)	CoV <sub>m</sub>	@25um %	@125um %	@150um %	25-125 yield* %	25-150 yield* %
1kg-0210-7	1	3060	4297	0.319	74.85	135.1	24.98	1.47	17.94	78.31	88.85	60.37	70.91
-0218-7	1	3050	4283	0.320	79.95	135.4	29.85	1.32	N/R	N/R	N/R	N/R	N/R
-0319-7	1	3050	4283	0.320	70.57	141	26.27	1.63	N/R	N/R	N/R	N/R	N/R
-0325-7	1	3000	4212	0.326	71.51	122.3	24.95	1.36	14.96	77.11	85.88	62.15	70.92
-0506-7	2	3560	4999	0.549	67.4	113.1	22.38	1.35	N/R	N/R	N/R	N/R	N/R
-0708-7	4	3260	3325	1.650	59.38	97.22	24.99	1.22	N/R	N/R	N/R	N/R	N/R
-0908-7	8	3140	3202	3.426	70.73	102.6	30.39	1.02	12.3	96.69	99.86	84.39	87.56
-1014-7	8	3030	3090	3.551	80.57	121	30.37	1.12	13	86.3	95.96	73.3	82.96
Average	1	3040	4268	0.321	74.22	133.5	26.51	1.44	16.45	77.71	87.37	61.26	70.92
Std. dev.		27	38	0.003	4.24	7.9	2.31	0.14	2.11	0.85	2.10	1.26	0.01
Average	8	3085	3146	3.489	75.65	111.80	30.38	1.07	12.65	91.50	97.91	78.85	85.26
Std. dev.		78	79	0.088	6.96	13.01	0.01	0.07	0.49	7.35	2.76	7.84	3.25

\* Theoretical yield based on the particle size analysis

Consistent with the 100 gram scale experiments, the results in Table 3 show that the width of the distribution of the microparticle size decreases with increasing residence time of the emulsion in the series of static mixers. As shown in Table 3, the average residence time for one static mixer was 0.321 sec, resulting in a CoV<sub>m</sub> of 1.44. Increasing the average residence time to 3.489 sec through the use of eight mixers, decreased the CoV<sub>m</sub> to 1.07. The longer average residence time also increased the

average yield in a desired microparticle size range of 25-125  $\mu\text{m}$  by 28.71%, and in a desired microparticle size range of 25-150  $\mu\text{m}$  by 20.22%.

The experiments and data described above demonstrate that the mass median diameter of the microparticles is inversely proportional to the average emulsion velocity through the static mixer. The experiments and data also demonstrate that the width of the microparticle size distribution ( $\text{CoV}_m$ ), and its symmetry, can be controlled by the residence time of the emulsion in the static mixer, or series of static mixers. Helical design static mixers, scissors design static mixers, and layered design static mixers all appear to behave similarly with respect to changes in velocity or residence time.

**Example 2 - Preparation of Risperidone Microparticles Using a Manifold**

Microparticles comprising risperidone were prepared at the 20-kilogram scale. The 20 Kg process (8 Kg of active agent and 12 Kg of polymer) provides a theoretical drug loading of the microparticles of 40% (8 Kg/20 Kg x 100%).

The polymer solution was prepared by dissolving 12.0 Kg of MEDISORB® 7525 DL polymer (Alkermes, Inc., Blue Ash, Ohio) in 60 Kg of ethyl acetate (Merck). The polymer was added to the solvent at 25°C in a stainless steel reactor. The temperature of the tank was raised to 37°C to facilitate dissolution. The vessel was agitated for at least 16 hours to dissolve the polymer. Once dissolved, the solution temperature was reduced to 25°C.

The drug solution was prepared by dissolving 8.0 Kg of risperidone base (Janssen Pharmaceutica, Beerse, Belgium) in 25.3 Kg of benzyl alcohol (Merck) at 25°C in a stainless steel reactor. The organic phase was prepared by adding the drug solution to the polymer solution at 25°C in a stainless steel reactor and mixing for at least 15 minutes.

The continuous or aqueous phase was prepared by dissolving 6.0 Kg of polyvinyl alcohol (PVA) (DuPont) in 594.0 Kg hot (>60°C) water for injection (WFI) in a stainless steel vessel to form a 1% solution. The vessel was agitated for at least 6 hours to dissolve the PVA. Once the PVA was dissolved, the temperature was reduced to 25°C and 42.0 Kg of ethyl acetate (Merck) was added, and mixed for at least 30 minutes to dissolve the ethyl acetate.



Using positive displacement pumps, the organic and aqueous phases were pumped through a static mixing assembly to form an oil-in-water emulsion. A preferred system for carrying out this process is shown in Figure 7. An organic phase 710 (polymer/drug solution) is pumped by a pump 712. A continuous phase 720 (PVA solution) is pumped by a pump 722. The organic and continuous phases are pumped into a static mixing assembly 730. Preferably, static mixing assembly 730 comprises a preblending static mixer 732 and a manifold 734. Manifold 734 preferably comprises a plurality of individual static mixers 736 configured to provide a plurality of parallel flow streams 738. Although Figure 7 shows two parallel flow streams in manifold 734, the present invention is not limited to the use of two flow streams, and more or less flow streams could be used in manifold 734, as would be readily apparent to one skilled in the art. Similarly, Figure 7 shows three individual static mixers 736 arranged in series to form flow streams 738. It should be readily apparent to one skilled in the art that other numbers, more or less, of static mixers 736 could be used to form flow streams 738.

The emulsion droplet size, and the resulting microparticle size, are controlled primarily by the flow rate and residence time through the static mixing assembly. The static mixing assembly used in the 20 Kg risperidone process consisted of a two inch diameter preblending static mixer upstream of a two flow stream manifold. Each flow stream in the manifold was formed by three, eighteen inch long, one inch diameter static mixers arranged in series. The larger diameter of the preblending static mixer is important to accommodate the total flow from the organic and aqueous phase feed streams at a lower velocity than the smaller diameter static mixers in the manifold.

The flow rates are set by nominal pump speed settings. The total flow rate was approximately 20-22 Kg/min, divided between the two flow streams in the manifold. The total flow rate can be divided one-half for each flow stream in the manifold, or in any other manner as would be readily apparent to one skilled in the art.

The flow rates for seven 20 Kg batches of microparticles are shown below in Table 4. In batches 03098, 03168, and 03238, the drug (risperidone) was not present, resulting in the production of "placebo" microparticles.

**Table 4** 20kg Emulsion flow rate summary

Batch	w/o ratio	Rate water	Rate oil	Rate Total
	w/w	kg/min	kg/min	kg/min
-03098	4.84	16.8	3.47	20.3
-03168	4.84	16.8	3.47	20.3
-03238	4.86	16.8	3.47	20.3
-03308	4.70	16.8	3.57	20.3
-04068	4.67	17.0	3.63	20.6
-04138	4.50	16.9	3.75	20.7
-04208	4.46	16.8	3.78	20.6
Average	4.7	16.8	3.6	20.4
SD	0.2	0.1	0.1	0.2

After exiting the static mixing assembly, the oil-in-water emulsion is transferred to a large agitated tank for solvent extraction or quench (extraction vessel 740 in Figure 7). The aqueous quench consisted of 4875 Kg WFI and 125 Kg ethyl acetate at 6°C. Solvents are extracted from the emulsion droplets, thereby hardening into microparticles. The microparticles were sampled from the extraction vessel and analyzed using a Coulter LQ100 particle size analyzer. The particle size results from these experiments are shown below in Table 5.

Batch #	Particle Size Characteristics		
	Mean (um)	Std. Dev.	% < 150um
0309-8	83.03	40.44	95.7
0316-8	80.14	43.79	94.5
0323-8	80.81	40.81	95.8
0330-8	82.24	36.9	97.7
0406-8	78.21	34.53	99
0413-8	80.47	35.31	98.5
0420-8	79.55	35.75	98.5
Average	80.64	38.22	97.10
Std. Dev	1.62	3.48	1.75

**Table 5**

As can be seen from Table 5, the percentage of microparticles within the desired microparticle size range of less than 150  $\mu$ m ranged from 94.5% to 99%, with an average of 97.1%. Through the use of the static mixing assembly, the particle size characteristics could be controlled to provide a desired microparticle size range.

It should be understood by one skilled in the art that the present invention is not limited to the use of an individual static mixer for any of the elements depicted as individual static mixers in the Figures. As would be readily apparent to one skilled in the art, a plurality of individual static mixers arranged in series could be used, or a manifold containing a plurality of individual static mixers arranged in series, or arranged in parallel to provide a plurality of parallel flow streams, could also be used.

### ***Example 3 – Methods for Preparing Microparticles***

As exemplified by the examples discussed above, methods for preparing microparticles in accordance with the present invention will now be described in more detail. In one embodiment of the present invention, a first phase, comprising an active agent and a polymer, is prepared. In one embodiment of the present invention, the first phase is prepared by dissolving the active agent in a first solvent to form an active agent solution. The polymer is dissolved in a second solvent to form a polymer solution. The active agent solution and the polymer solution are blended to form the first phase. In a particularly preferred embodiment, the active agent is selected from the group consisting of risperidone, 9-hydroxyrisperidone, and pharmaceutically acceptable salts thereof. In such an embodiment, a preferred first solvent is benzyl alcohol, and a preferred second solvent is ethyl acetate.

In another embodiment of the present invention, the first phase is prepared by dissolving the active agent and the polymer in a solvent to form a solution. In a particularly preferred embodiment, the active agent is bupivacaine, and the solvent is ethyl acetate. It should be understood that the present invention is not limited to any particular method or process by which the first phase is prepared, and other suitable processes would be readily apparent to one skilled in the art.

A second phase is prepared, and combined with the first phase in a first static mixer to form an emulsion. In a preferred embodiment, the two phases are pumped into the static mixer, with the second phase being pumped at a flow rate greater than the flow rate of the first phase. In one preferred embodiment, the ratio of the flow rate of the second phase to the flow rate of the first phase is from about 4:1 to about 5:1. However, it

should be understood by one skilled in the art that the present invention is not limited to such a flow rate ratio, and other appropriate flow rate ratios would be readily apparent to one skilled in the art.

5 The emulsion flows through a manifold that includes a plurality of static mixers into a quench liquid whereby droplets of the emulsion form microparticles. The quench liquid is prepared in a manner well known to one skilled in the art. The quench may be water, such as WFI or it may be an aqueous solution comprising one or more solvents.

10 Preferably, the diameter of the first static mixer is greater than the diameter of each of the plurality of static mixers in the manifold. In one embodiment, the plurality of static mixers is configured to provide a plurality of parallel flow streams. In a particularly preferred embodiment, the plurality of static mixers in the manifold is two. However, it should be understood by one skilled in the art that the present invention is not limited to the use of two static mixers in such a configuration, and other appropriate numbers of static mixers would be readily apparent to one skilled in the art.

15 Alternatively, the plurality of static mixers can be configured in series to provide a plurality of sequential flow streams.

The step of flowing the emulsion through the manifold is preferably performed by flowing a portion of a total flow rate through each of the static mixers in the manifold, the total flow rate being the sum of the flow rate of the first phase and the flow rate of the

20 second phase. For example, for a manifold configured with two static mixers, a portion of the total flow rate will flow through each of the two static mixers. The portion flowing through each of the two static mixers can be one-half, or other portions as would be readily apparent to one skilled in the art.

An alternate method for preparing microparticles in accordance with the present

25 invention will now be described. A first phase, comprising an active agent and a polymer, is prepared. A second phase is prepared, and combined with the first phase in a first static mixer to form an emulsion, the emulsion forming an outflow of the first static mixer. Suitable methods and processes for preparing the first and second phases, and for combining in the first static mixer, have been described above and will not be repeated

30 here for brevity.

The outflow of the first static mixer is divided to form at least two flow streams. Each of the at least two flow streams flows through a separate second static mixer. The separate second static mixer can be an individual static mixer, one of a plurality of individual static mixers arranged in series, or one of a plurality of individual static mixers configured to provide a plurality of parallel flow streams. Preferably, the diameter of the first static mixer is greater than the diameter of each separate second static mixer. The at least two flow streams may have substantially equal flow rates, or such other flow rates as would be apparent to one skilled in the art.

The at least two flow streams are combined with a quench liquid whereby droplets of the emulsion form microparticles. The quench liquid can be the same as, or different from, the second phase.

A method for controlling particle size distribution of microparticles in accordance with the present invention will now be described. In a manner as described above, a first phase, comprising an active agent and a polymer, is prepared. A second phase is prepared, and combined with the first phase in a static mixing assembly to form an emulsion. The emulsion flows into a quench liquid whereby droplets of the emulsion form microparticles. The residence time of the emulsion in the static mixing assembly is adjusted to obtain a predetermined particle size distribution of the resulting microparticles. The residence time is equal to a length of the static mixing assembly divided by an average velocity of the emulsion through the static mixing assembly. Increasing the residence time of the emulsion in the static mixing assembly narrows the particle size distribution. Similarly, decreasing the residence time of the emulsion in the static mixing assembly broadens the particle size distribution. The residence time may be adjusted by changing the length of the static mixing assembly. In one embodiment, the residence time is from about three seconds to about four seconds. However, it should be understood by one skilled in the art that the present invention is not limited to such a residence time, and other residence times may be used.

In one embodiment of the present invention, the static mixing assembly comprises a plurality of individual static mixers configured so that the emulsion flows sequentially through the plurality of individual static mixers. In an alternate embodiment, the static

mixing assembly comprises a first static mixer and a manifold, in fluid communication with the first static mixer, which includes a plurality of static mixers. In such an alternate embodiment, the diameter of the first static mixer is preferably greater than the diameter of each of the plurality of static mixers in the manifold.

5 ***Microparticles of the Present Invention***

The microparticles prepared by the process of the present invention preferably comprise a polymeric binder, but it should be understood by one skilled in the art that the present invention is not limited to preparation of microparticles comprising a polymeric binder. Suitable polymeric binder materials include poly(glycolic acid), poly-d,l-lactic  
10 acid, poly-l-lactic acid, copolymers of the foregoing, poly(aliphatic carboxylic acids), copolyoxalates, polycaprolactone, polydioxanone, poly(ortho carbonates), poly(acetals), poly(lactic acid-caprolactone), polyorthoesters, poly(glycolic acid-caprolactone), polyanhydrides, polyphosphazines, albumin, casein, and waxes. Poly (d,l-lactic-co-glycolic acid) is commercially available from Alkermes, Inc. (Blue Ash, OH). A suitable  
15 product commercially available from Alkermes, Inc. is a 50:50 poly(d,l-lactic-co-glycolic acid) known as MEDISORB® 5050 DL. This product has a mole percent composition of 50% lactide and 50% glycolide. Other suitable commercially available products are MEDISORB® 6535 DL, 7525 DL, 8515 DL and poly(d,l-lactic acid) (100 DL). Poly(lactide-co-glycolides) are also commercially available from Boehringer Ingelheim  
20 (Germany) under its Resomer® mark, e.g., PLGA 50:50 (Resomer® RG 502), PLGA 75:25 (Resomer® RG 752) and d,l-PLA (Resomer® RG 206), and from Birmingham Polymers (Birmingham, Alabama). These copolymers are available in a wide range of molecular weights and ratios of lactic acid to glycolic acid.

One type of microparticle suitable for preparation by the present invention is a  
25 sustained-release microparticle that is biodegradable. However, it should be understood by one skilled in the art that the present invention is not limited to biodegradable or other types of sustained-release microparticles. As would be apparent to one skilled in the art, the molecular weight of the polymeric binder material for biodegradable microparticles is of some importance. The molecular weight should be high enough to permit the

formation of satisfactory polymer coatings, i.e., the polymer should be a good film former. Usually, a satisfactory molecular weight is in the range of 5,000 to 500,000 daltons, preferably about 150,000 daltons. However, since the properties of the film are also partially dependent on the particular polymeric binder material being used, it is very  
5 difficult to specify an appropriate molecular weight range for all polymers. The molecular weight of the polymer is also important from the point of view of its influence upon the biodegradation rate of the polymer. For a diffusional mechanism of drug release, the polymer should remain intact until all of the drug is released from the microparticles and then degrade. The drug can also be released from the microparticles  
10 as the polymeric binder bioerodes. By an appropriate selection of polymeric materials a microparticle formulation can be made in which the resulting microparticles exhibit both diffusional release and biodegradation release properties. This is useful in according multiphasic release patterns.

The microparticles prepared in accordance with the present invention may include  
15 an active agent or other type of substance that is released from the microparticles into the host. Such active agents can include 1,2-benzazoles, more particularly, 3-piperidinyl-substituted 1,2-benzisoxazoles and 1,2-benzisothiazoles. The most preferred active agents of this kind are 3-[2-[4-(6-fluoro-1,2-benzisoxazol-3-yl)-1-piperidinyl]ethyl]-6,7,8,9-tetrahydro-2-methyl-4H--pyrido[1,2-a]pyrimidin-4-one ("risperidone") and 3-[2-  
20 [4-(6-fluoro-1,2-benzisoxazol-3-yl)-1-piperidinyl]ethyl]-6,7,8,9-tetrahydro-9-hydroxy-2-methyl-4H--pyrido[1,2-a]pyrimidin-4-one ("9-hydroxyrisperidone") and the pharmaceutically acceptable salts thereof. Risperidone (which term, as used herein, is intended to include its pharmaceutically acceptable salts) is most preferred. Risperidone can be prepared in accordance with the teachings of U.S. Patent No. 4,804,663, the  
25 entirety of which is incorporated herein by reference. 9-hydroxyrisperidone can be prepared in accordance with the teachings of U.S. Patent No. 5,158,952, the entirety of which is incorporated herein by reference.

Other biologically active agents include non-steroidal antifertility agents; parasympathomimetic agents; psychotherapeutic agents; major tranquilizers such as  
30 chlorpromazine HCl, clozapine, mesoridazine, metiapine, reserpine, thioridazine and the

like; minor tranquilizers such as chlordiazepoxide, diazepam, meprobamate, temazepam and the like; rhinological decongestants; sedative-hypnotics such as codeine, phenobarbital, sodium pentobarbital, sodium secobarbital and the like; steroids such as testosterone and testosterone propionate; sulfonamides; sympathomimetic agents; 5 vaccines; vitamins and nutrients such as the essential amino acids; essential fats and the like; antimalarials such as 4-aminoquinolines, 8-aminoquinolines, pyrimethamine and the like; anti-migraine agents such as mazindol, phentermine and the like; anti-Parkinson agents such as L-dopa; anti-spasmodics such as atropine, methscopolamine bromide and the like; antispasmodics and anticholinergic agents such as bile therapy, digestants, 10 enzymes and the like; antitussives such as dextromethorphan, noscapine and the like; bronchodilators; cardiovascular agents such as anti-hypertensive compounds, Rauwolfia alkaloids, coronary vasodilators, nitroglycerin, organic nitrates, pentaerythritotetranitrate and the like; electrolyte replacements such as potassium chloride; ergotalkaloids such as ergotamine with and without caffeine, hydrogenated ergot alkaloids, dihydroergocristine 15 methanesulfate, dihydroergocornine methanesulfonate, dihydroergokryptine methanesulfate and combinations thereof; alkaloids such as atropine sulfate, Belladonna, hyoscyne hydrobromide and the like; analgetics, narcotics such as codeine, dihydrocodienone, meperidine, morphine and the like; non-narcotics such as salicylates, aspirin, acetaminophen, d-propoxyphene and the like; antibiotics such as salicylates, 20 aspirin, acetaminophen, d-propoxyphene and the like; antibiotics such as the cephalosporins, chloramphenicol, gentamicin, Kanamycin A, Kanamycin B, the penicillins, ampicillin, streptomycin A, antimycin A, chloropamtheniol, metromidazole, oxytetracycline, penicillin G, the tetracyclines, and the like; anti-cancer agents; anti-convulsants such as mephenytoin, phenobarbital, trimethadione; anti-emetics such as 25 thiethylperazine; antihistamines such as chlorophenazine, dimenhydrinate, diphenhydramine, perphenazine, tripelemamine and the like; anti-inflammatory agents such as hormonal agents, hydrocortisone, prednisolone, prednisone, non-hormonal agents, allopurinol, aspirin, indomethacin, phenylbutazone and the like; prostaglandins; cytotoxic drugs such as thiopeta; chlorambucil, cyclophosphamide, melphalan, nitrogen 30 mustard, methotrexate and the like; antigens of such microorganisms as *Neisseria*



gonorrhea, *Mycobacterium tuberculosis*, Herpes virus (homonis, types 1 and 2), *Candida albicans*, *Candida tropicalis*, *Trichomonas vaginalis*, *Haemophilus vaginalis*, Group B *Streptococcus coli*, *Mycoplasma hominis*, *Haemophilus ducreyi*, *Granuloma inguinale*, *Lymphopathia venereum*, *Treponema pallidum*, *Brucella abortus*, *Brucella melitensis*,  
5 *Brucella suis*, *Brucella canis*, *Campylobacter fetus*, *Campylobacter fetus intestinalis*, *Leptospira pomona*, *Listeria monocytogenes*, *Brucella ovis*, Equine herpes virus 1, Equine arteritis virus, IBR-IBP virus, BVD-MB virus, *Chlamydia psittaci*, *Trichomonas foetus*, *Toxoplasma gondii*, *Escherichia coli*, *Actinobacillus equuli*, *Salmonella abortus ovis*, *Salmonella abortus equi*, *Pseudomonas aeruginosa*, *Corynebacterium equi*,  
10 *Corynebacterium pyogenes*, *Actinobacillus seminis*, *Mycoplasma bovigenitalium*, *Aspergillus fumigatus*, *Absidia ramosa*, *Trypanosoma equiperdum*, *Babesia caballi*, *Clostridium tetani*, and the like; antibodies that counteract the above microorganisms; and enzymes such as ribonuclease, neuramidinase, trypsin, glycogen phosphorylase, sperm lactic dehydrogenase, sperm hyaluronidase, adenosinetriphosphatase, alkaline  
15 phosphatase, alkaline phosphatase esterase, amino peptidase, trypsin, chymotrypsin, amylase, muramidase, acrosomal proteinase, diesterase, glutamic acid dehydrogenase, succinic acid dehydrogenase, beta-glycophosphatase, lipase, ATP-ase alpha-peptate gamma-glutamylotranspeptidase, sterol-3-beta-ol-dehydrogenase, and DPN-di-aprorasse.

Other suitable active agents include estrogens such as diethyl stilbestrol, 17-beta-  
20 estradiol, estrone, ethinyl estradiol, mestranol, and the like; progestins such as norethindrone, norgestryl, ethynodiol diacetate, lynestrenol, medroxyprogesterone acetate, dimethisterone, megestrol acetate, chlormadinone acetate, norgestimate, norethisterone, ethisterone, melengestrol, norethynodrel and the like; and the spermicidal compounds such as nonylphenoxypolyoxyethylene glycol, benzethonium chloride,  
25 chlorindanol and the like.

Still other suitable active agents include antifungals, antivirals, anticoagulants, anticonvulsants, antidepressants, antihistamines, hormones, vitamins and minerals, cardiovascular agents, peptides and proteins, nucleic acids, immunological agents, antigens of such bacterial organisms as *Streptococcus pneumoniae*, *Haemophilus*  
30 *influenzae*, *Staphylococcus aureus*, *Streptococcus pyogenes*, *Corynebacterium*

*diphtheriae*, *Bacillus anthracis*, *Clostridium tetani*, *Clostridium botulinum*, *Clostridium perfringens*, *Streptococcus mutans*, *Salmonella typhi*, *Haemophilus parainfluenzae*, *Bordetella pertussis*, *Francisella tularensis*, *Yersinia pestis*, *Vibrio cholerae*, *Legionella pneumophila*, *Mycobacterium leprae*, *Leptospira interrogans*, *Borrelia burgdorferi*,  
5 *Campylobacter jejuni*, antigens of such viruses as smallpox, influenza A and B, respiratory syncytial, parainfluenza, measles, HIV, varicella-zoster, herpes simplex 1 and 2, cytomegalovirus, Epstein-Barr, rotavirus, rhinovirus, adenovirus, papillomavirus, poliovirus, mumps, rabies, rubella, coxsackieviruses, equine encephalitis, Japanese encephalitis, yellow fever, Rift Valley fever, lymphocytic choriomeningitis, hepatitis B,  
10 antigens of such fungal protozoan, and parasitic organisms such as *Cryptococcus neoformans*, *Histoplasma capsulatum*, *Candida albicans*, *Candida tropicalis*, *Nocardia asteroides*, *Rickettsia rickettsii*, *Rickettsia typhi*, *Mycoplasma pneumoniae*, *Chlamydia psittaci*, *Chlamydia trachomatis*, *Plasmodium falciparum*, *Trypanosoma brucei*, *Entamoeba histolytica*, *Toxoplasma gondii*, *Trichomonas vaginalis*, *Schistosoma*  
15 *mansoni*. These antigens may be in the form of whole killed organisms, peptides, proteins, glycoproteins, carbohydrates, or combinations thereof.

Still other macromolecular bioactive agents that may be chosen for incorporation include, but are not limited to, blood clotting factors, hemopoietic factors, cytokines, interleukins, colony stimulating factors, growth factors, and analogs and fragments  
20 thereof.

The microparticles can be mixed by size or by type. However, it should be understood that the present invention is not limited to the use of biodegradable or other types of microparticles that contain an active agent. In one embodiment, the microparticles are mixed in a manner that provides for the delivery of active agent to the  
25 patient in a multiphasic manner and/or in a manner that provides different active agents to the patient at different times, or a mixture of active agents at the same time. For example, secondary antibiotics, vaccines, or any desired active agent, either in microparticle form or in conventional, unencapsulated form can be blended with a primary active agent and provided to the patient.

### ***Conclusion***

While various embodiments of the present invention have been described above, it should be understood that they have been presented by way of example only, and not limitation. The present invention is not limited to the preparation of controlled release  
5 microparticles, nor is it limited to a particular active agent, polymer or solvent, nor is the present invention limited to a particular scale or batch size. The present invention is not limited to any type or design of static mixer. Thus, the breadth and scope of the present invention should not be limited by any of the above-described exemplary embodiments, but should be defined only in accordance with the following claims and their equivalents.